



## **I filtri: istruzioni per l'uso corretto**

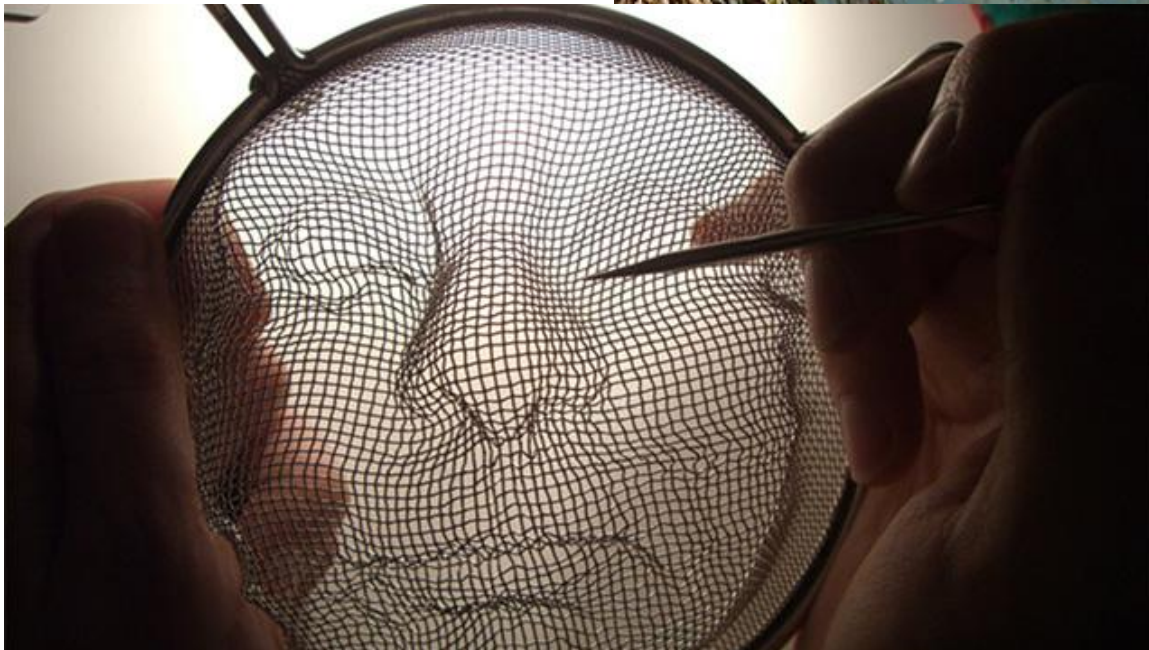
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**Direttore UOC Cardiologia**

**A.O. Ospedale San Carlo Borromeo Milano**



# Il filtro



# I Filtri

- **L'ECG è la registrazione, nel tempo, dell'attività elettrica del cuore.**
- **La sequenza cardiaca ha una natura elettrica ed è possibile misurare questa azione elettro-chimica direttamente sulla superficie corporea (visto che il corpo è conduttivo).**
- **Durante la propagazione dell'impulso nelle diverse parti del cuore, i fenomeni di depolarizzazione e ripolarizzazione generano campi elettrici che si estendono alla superficie del corpo.**

# I filtri

- **Le variazioni istantanee di grandezza e direzione di questi campi elettrici si rispecchiano in variazioni delle differenze di potenziale, che possono essere misurate tra punti diversi della superficie corporea.**
- **Un potenziale elettrico all'incirca di 1mV si sviluppa tra diversi punti della superficie corporea, ed è possibile misurarlo posizionando degli elettrodi direttamente a contatto con la pelle**

# I filtri: problemi tecnici

- Correnti a livello dell'interfaccia elettrodo esplorante/cute, corrente di alimentazione, correnti del sistema di amplificazione del segnale
- Una regola fondamentale nella misurazione è non permettere che uno strumento di misura influenzi il segnale sotto osservazione. Un amplificatore dovrebbe esibire un'alta impedenza di ingresso per far sì che non vengano attenuati i segnali fisiologici che si stanno misurando.
- Nel caso del segnale elettrocardiografico, l'elettrodo stesso dell'ECG ha una bassa impedenza, ma l'impedenza della pelle, può variare da  $100\Omega$  ad  $1\text{ M}\Omega$ . Le correnti d'ingresso dell'amplificatore generano potenziali ai capi dell'impedenza della pelle, che sono amplificate dal guadagno dell'amplificatore, causando elevati offset in DC nell'uscita dell'amplificatore.

# I filtri: problemi tecnici

- Il problema diventa grave quando i biopotenziali, che vogliamo monitorare, hanno un'energia utile che assume valori in un intervallo di **50/60 Hz**.
- **Rumore e deriva.**

Sono i segnali indesiderati che contaminano le misurazioni fisiologiche, il rumore prodotto all'interno della circuiteria dell'amplificatore è di solito definito, come quel segnale con componenti al di sopra di **0,1 Hz**, mentre deriva si riferisce alle variazioni della linea di base (baseline) al di sotto di **0.1 Hz**

# I filtri

- **La larghezza di banda di un amplificatore fisiologico dovrebbe essere in grado di amplificare correttamente tutte le frequenze significative nel segnale, mentre dovrebbe reiettare quei segnali fuori dalla banda d'interesse.**
- **La larghezza di banda è definita come la differenza tra la frequenza di taglio inferiore e la frequenza di taglio superiore.**



# I filtri

## Grandezze tipiche ECG

Amplificazione di un fattore all'incirca 1000 (60db) solo nella banda utile (il segnale originale ECG è dell'ordine di circa 1-5 mV)

- Per il monitoraggio freq. comprese 0.05 – 50 Hz
- Per la diagnostica freq. fino al 1KHz

Alta impedenza d'ingresso per evitare che l'impedenza incognita dell'elettrodo possa creare una partizione del segnale, attenuandolo

**Deve reiettare un forte disturbo della rete (50Hz) di ampiezza paragonabile al segnale (filtro Notch)**

A norma di legge la corrente che circola sul paziente deve essere inferiore a  $10\mu\text{A}$  (correnti superiori aumentano l'incidenza di Fibrillazione)

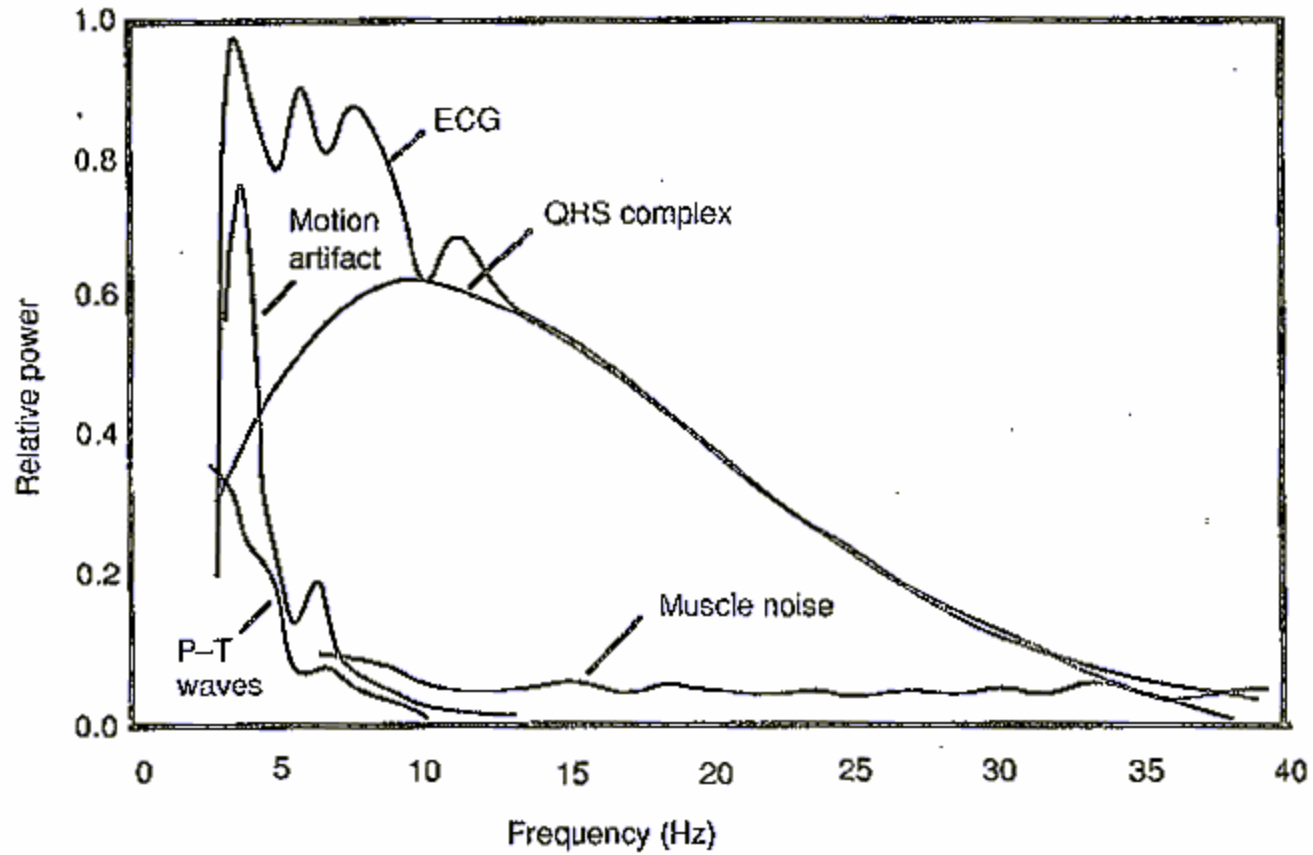
# I filtri

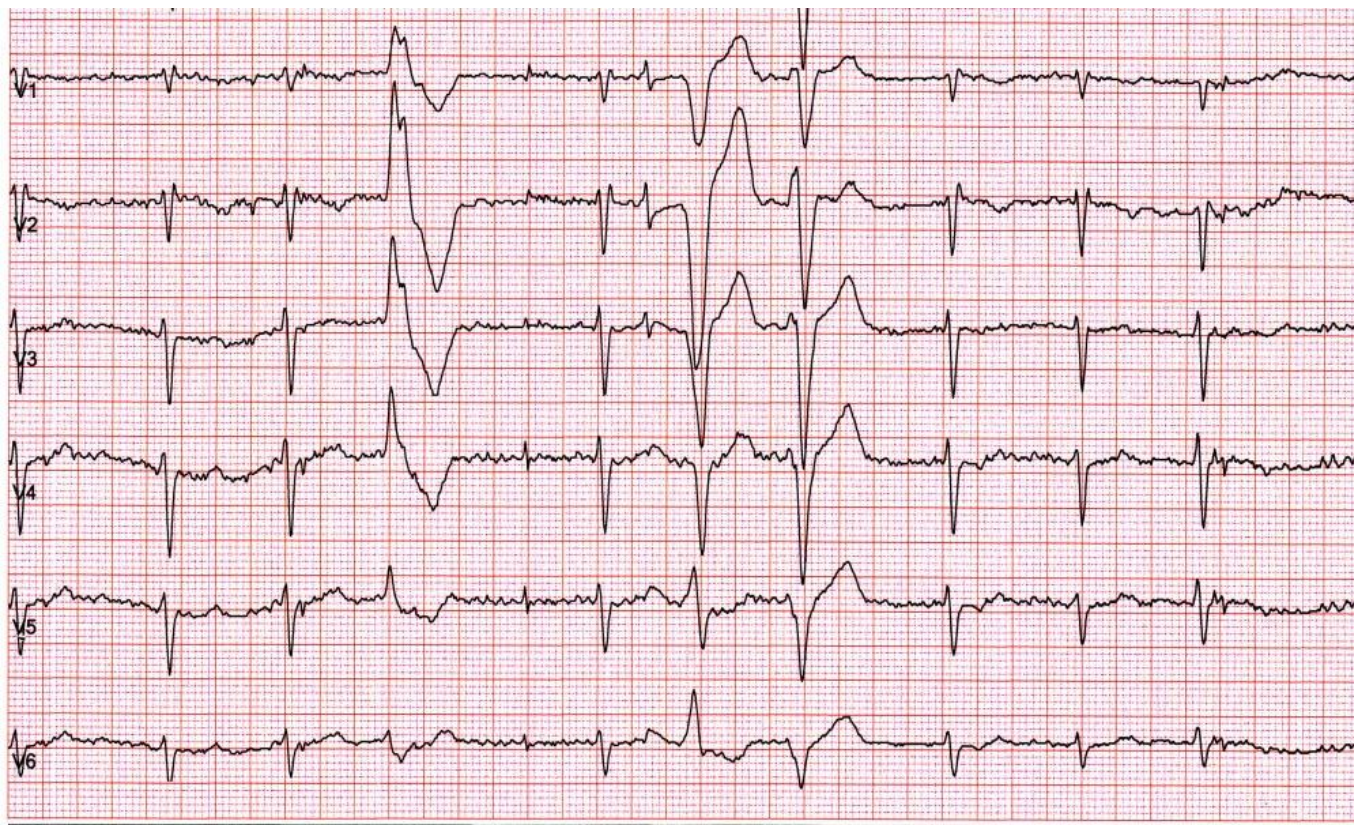
- **il QRS ha un contenuto in freq. più alto (picco 10-15 Hz) rispetto alle onde P e T (4-5 Hz)**
- **artefatti da movimento (contatti elettrodi) sono a bassa frequenza**
- **Molti segnali dell'attività fisiologica hanno ampiezze piccole e devono essere amplificati e processati prima che possano essere considerati in maniera significativa con l'utilizzo di amplificatori biopotenziali**

# I filtri: problemi tecnici

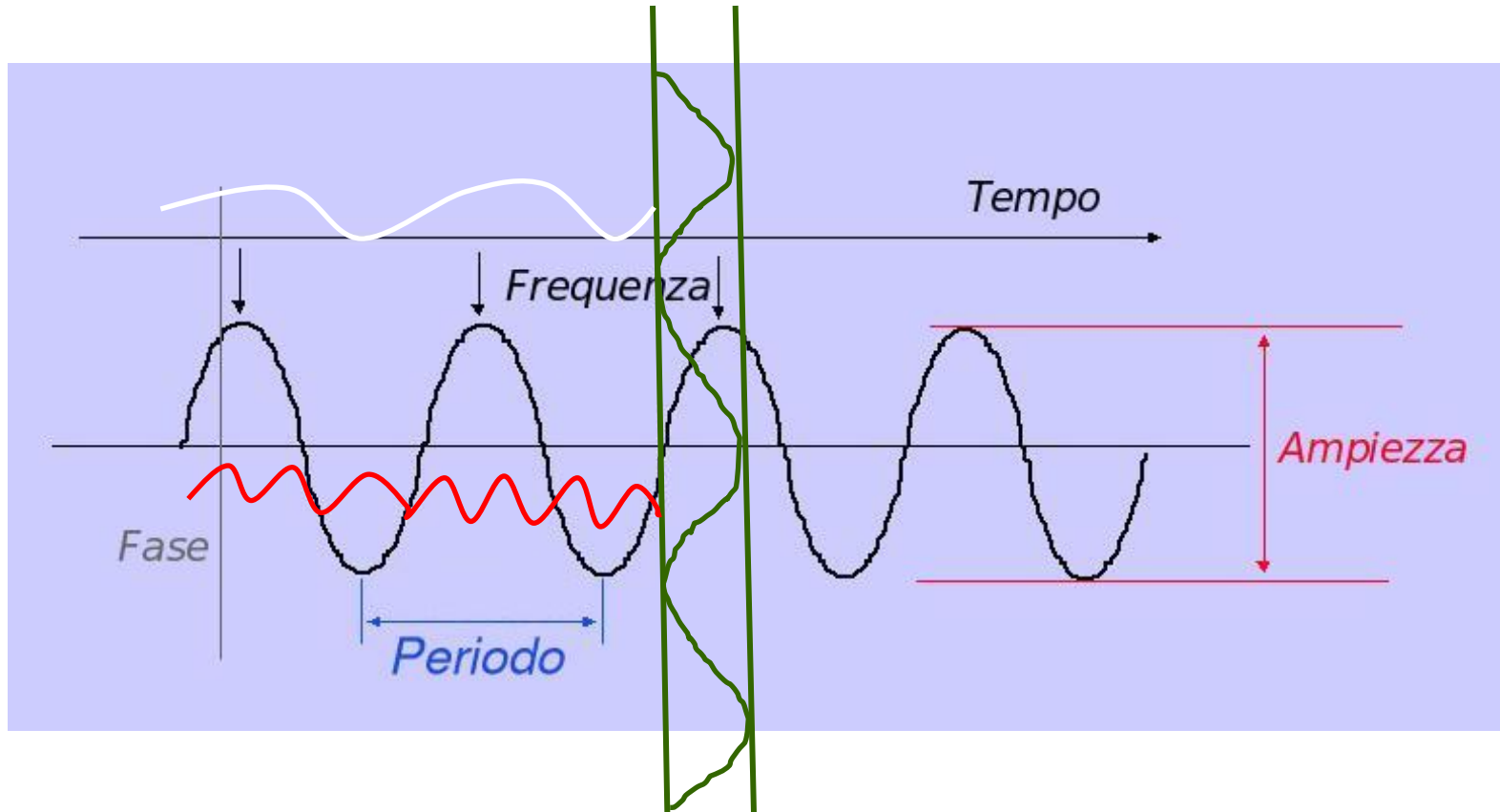
- Il complesso QRS può oscillare tra  $400\mu\text{V}$  a  $2,5\text{mV}$ , e richiede un guadagno in tensione che va da 100 a 1000. La **banda dell'ECG** è stata **standardizzata** per rendere uniforme l'interpretazione dei risultati. Vengono usati due filtri con banda a -3 dB (guadagno), un filtro passa alto a **0.05 Hz** e un filtro passa basso a **150 Hz**. Risposta in frequenza
- Ci sono molti altri potenziali che sono inavvertitamente amplificati usando elettrodi per monitorare l'ECG. La potenza condotta produce un alto livello di interferenze elettromagnetiche (EM), che devono essere accuratamente eliminate. Il corpo umano è una buona antenna
- Altre fonti di radiazioni EM sono le stazioni radio, cellulari, telefoni portatili, sorgenti a microonde, computer.

# I filtri



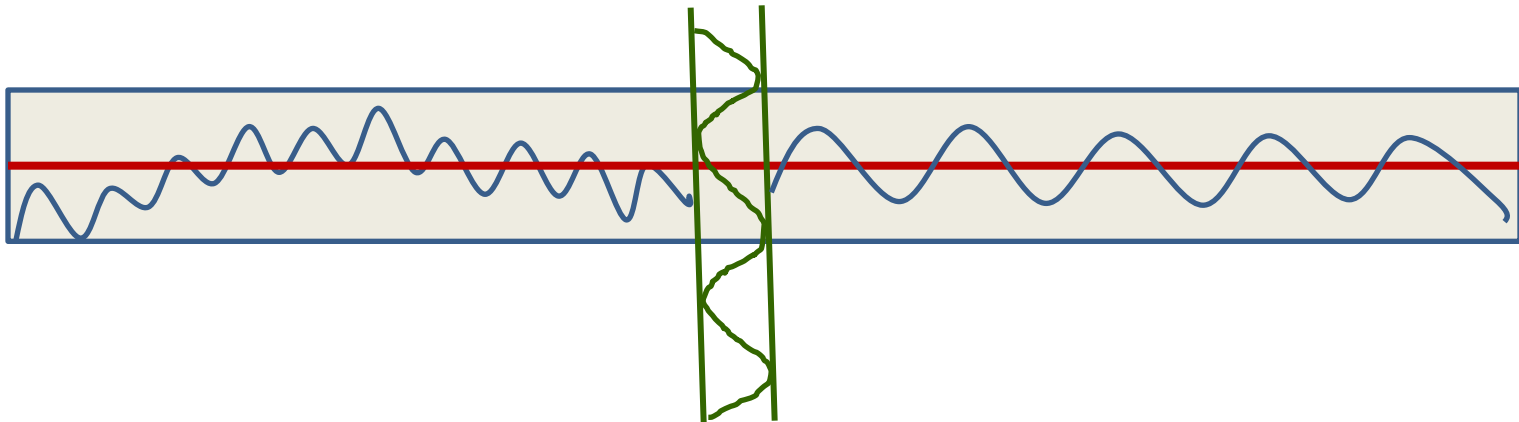
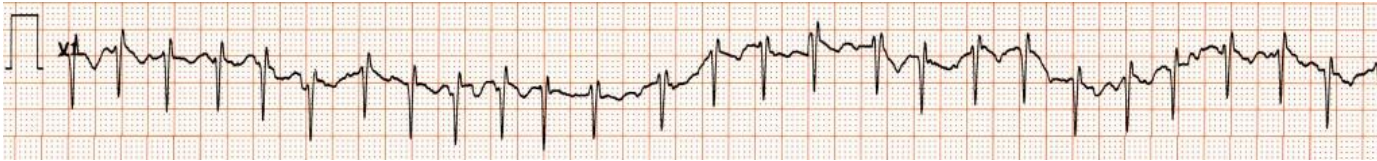


# Perché Il filtro

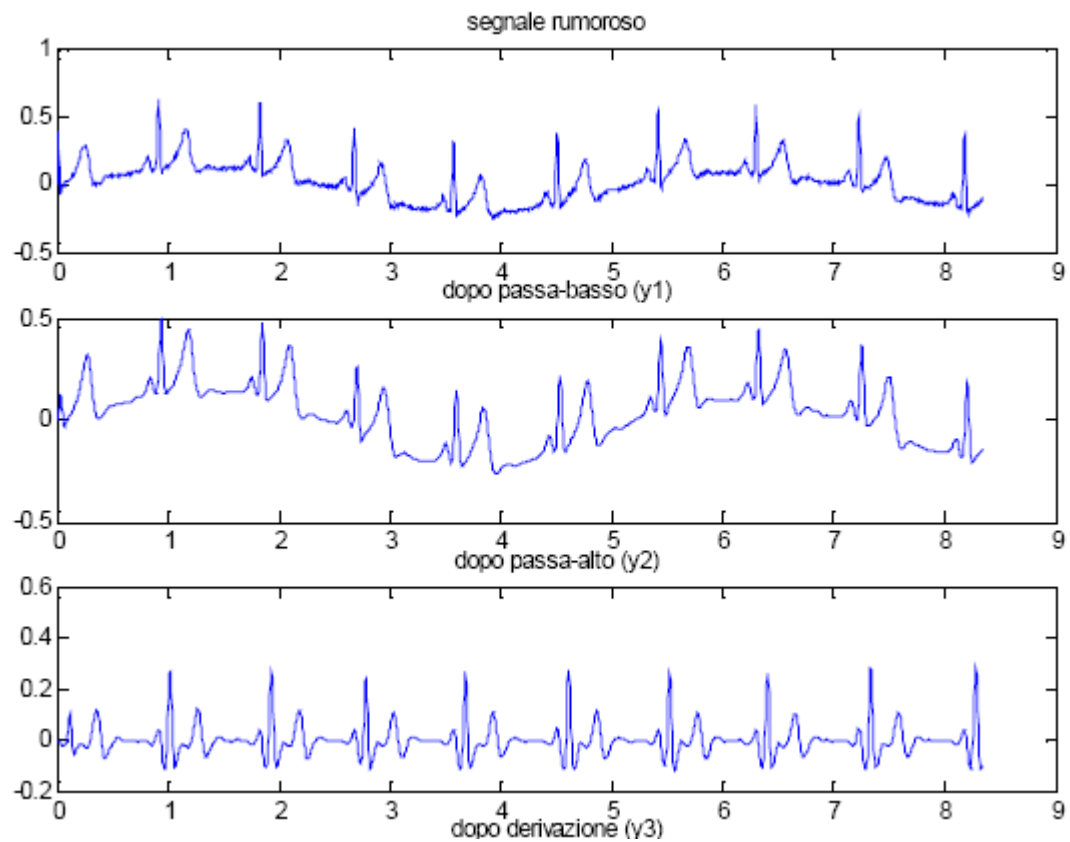


**L'elettrocardiografo è in grado di registrare tutte le correnti generate alla superficie del corpo, non solo quella dell'attività elettrica del cuore**

# Perché Il filtro

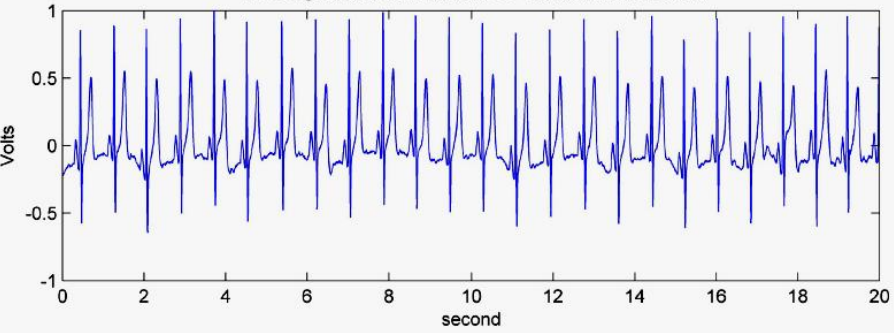


**L'elettrocardiografo è in grado di registrare anche le oscillazioni rispetto alla linea di base legate alla instabilità del segnale (wandering, tipicamente legato al respiro)**

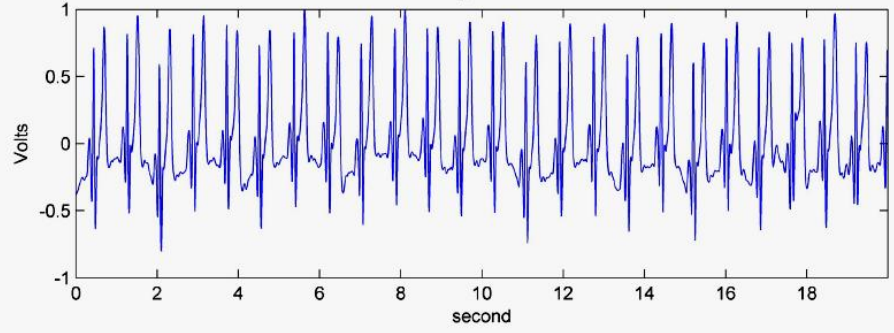




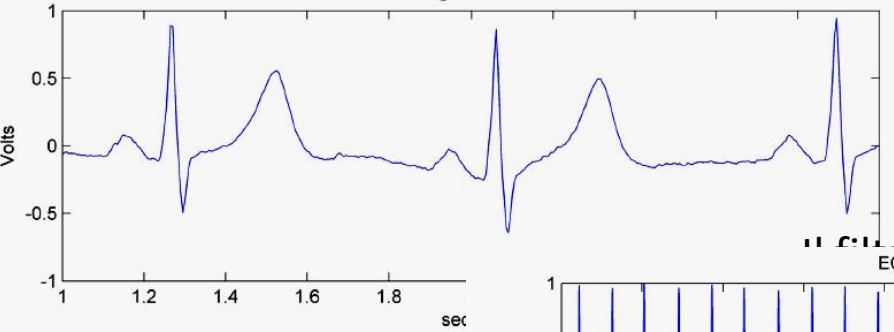
ECG Signal after cancellation DC drift and normalization



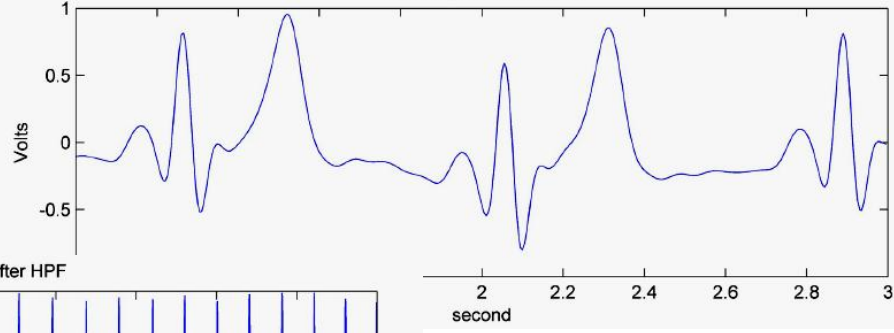
ECG Signal after LPF



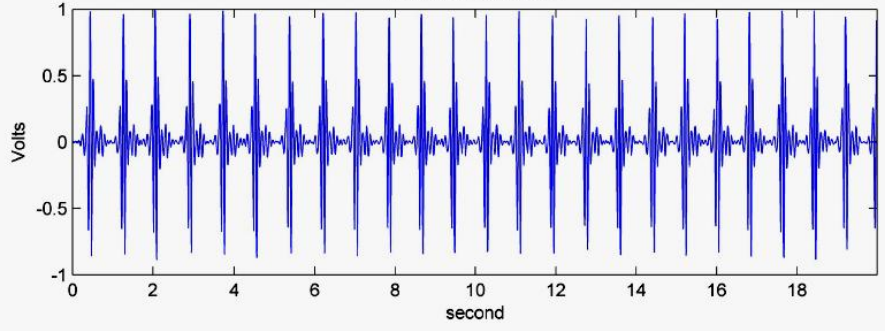
ECG Signal 1-3 second



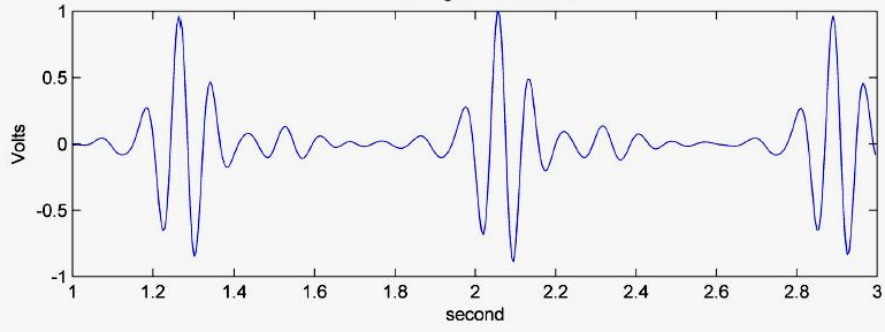
ECG Signal 1-3 second



ECG Signal after HPF



ECG Signal 1-3 second



## Prevalence and Clinical Implications of Improper Filter Settings in Routine Electrocardiography

**Only 25% of ECGs** (65 of 256) conformed to recommended standards; 75% of ECGs (191 of 254) did not. The most prevalent deviation from standard was **reduced high-frequency cutoff**, which was present in **96%** of tracings with nonstandard bandwidth (most commonly 40 Hz). **Increased low-frequency** cutoff was present in **62%** of ECGs in which it was documented

# **Recommendations for the Standardization and Interpretation of the Electrocardiogram**

## **Part I: The Electrocardiogram and Its Technology**

**A Scientific Statement From the American Heart Association  
Electrocardiography and Arrhythmias Committee, Council on Clinical  
Cardiology; the American College of Cardiology Foundation; and the  
Heart Rhythm Society**

*Endorsed by the International Society for Computerized Electrocardiology*

**This statement examines the relation of the resting ECG to its technology. Its purpose is to foster understanding of how the modern ECG is derived and displayed and to establish standards that will improve the accuracy and usefulness of the ECG in practice. Derivation of representative waveforms and measurements based on global intervals are described. Special emphasis is placed on digital signal acquisition and computer-based signal processing, which provide automated measurements that lead to computer-generated diagnostic statements. Lead placement, recording methods, and waveform presentation are reviewed. Throughout the statement, recommendations for ECG standards are placed in context of the clinical implications of evolving ECG technology.**

## **Recommendations for the Standardization and Interpretation.....**

- The fundamental frequency for the QRS complex at the body surface is  $\approx 10$  Hz, and most of the diagnostic information is contained below 100 Hz in adults, although low-amplitude, high-frequency components as high as 500 Hz have been detected and studied.**
- The QRS of infants often contains important components as high as 250 Hz. The fundamental frequency of T waves is approximately 1 to 2Hz.**

# Recommendations for the Standardization and Interpretation.....

- Filtering of the ECG signal to within the band between 1 to 30 Hz produces a stable ECG that is generally free of artifact, but this bandwidth is unacceptable for diagnostic recording because it produces distortions of both high- and low-frequency components of the signal.
- The **high-frequency** components of the ECG signal define the most rapidly changing parts of the signal, including **Q waves** and **notched components within the QRS** complex. Because QRS amplitude measurement depends on accurate detection of the peak of an R wave, an inadequate high-frequency response results in **systematic underestimation** of signal **amplitude** and in **smoothing of notches and Q waves**.

# **I filtri: problemi tecnici**

## **Low-Frequency Filtering**

**The heart rate, in beats (cycles) per minute (bpm), when divided by 60 (seconds per minute) forms a lower bound for the frequency content in Hertz (Hz, cycles per second). In practice, this is unlikely to be lower than 0.5 Hz, which corresponds to a heart rate of 30 bpm; heart rates below 40 bpm (0.67 Hz) are uncommon in practice. However, with traditional analog filtering, a 0.5-Hz low-frequency cutoff introduces considerable distortion into the ECG, particularly with respect to the level of the ST segment**

# I filtri: problemi tecnici

- **This distortion results from phase nonlinearities that occur in areas of the ECG signal where frequency content and wave amplitude change abruptly, as occurs where the end of the QRS complex meets the ST segment. Digital filtering provides methods for increasing the low-frequency cutoff without the introduction of phase distortion.**

# **Recommendations for the Standardization and Interpretation.....**

- **On the other hand, an inadequate low-frequency response can result in important distortions of repolarization. Accordingly, the transfer functions of the filtering algorithms of analog and digital electrocardiographs have a major effect on the resulting ECG.**
- **the digital ECG must eliminate or suppress low-frequency noise that results from baseline wander, movement, and respiration and higher-frequency noise that results from muscle artifact and power-line or radiated electromagnetic interference**



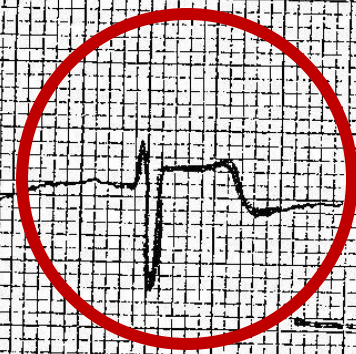
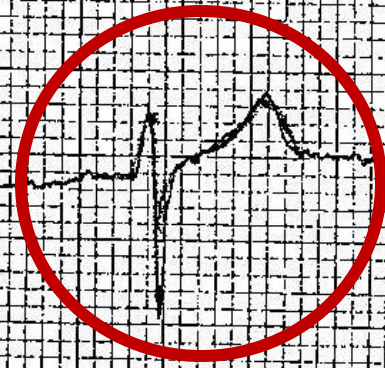
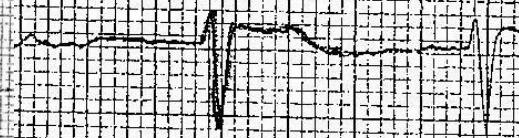
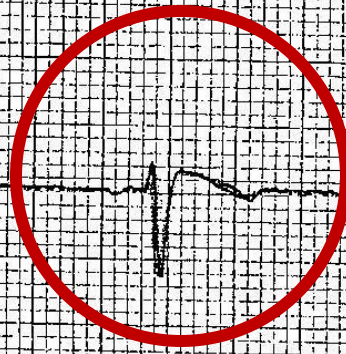
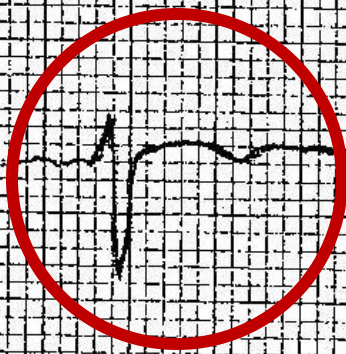
IV1

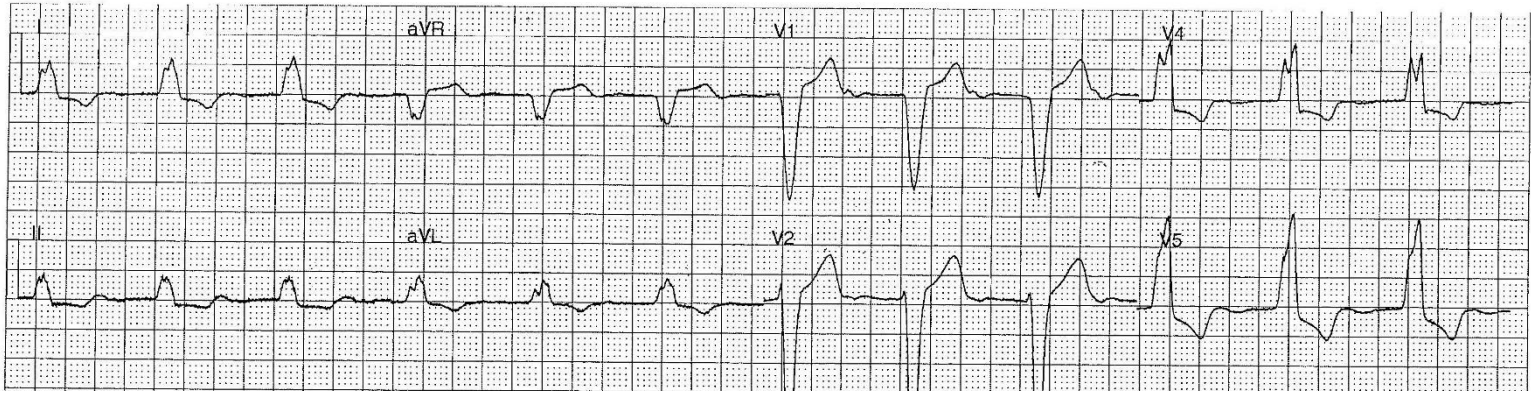
IV4

15:49:26 FC:72

IV5

IV6

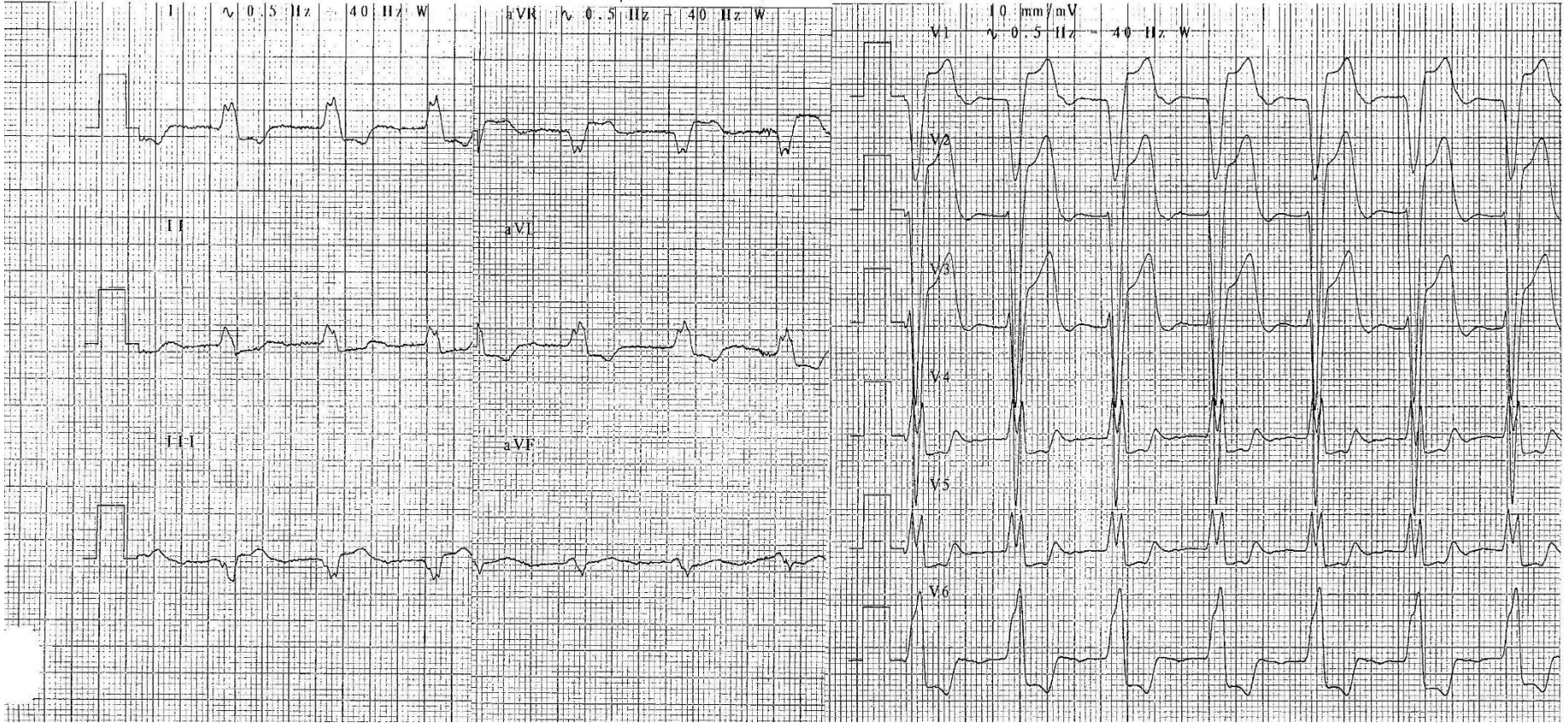




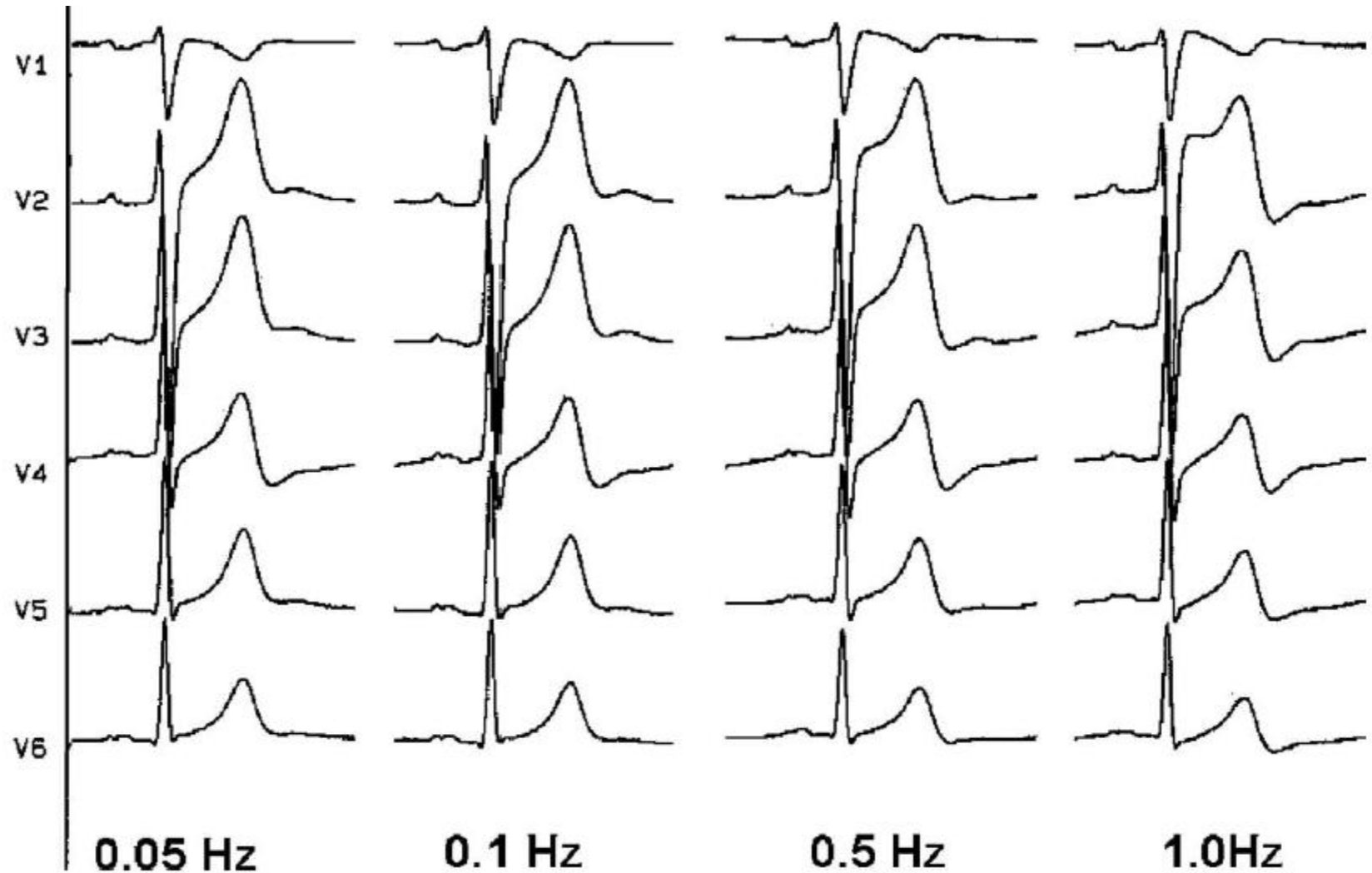
25 mm/s  
10 mm/mV

25 mm/s  
10 mm/mV

25 mm/s  
10 mm/mV

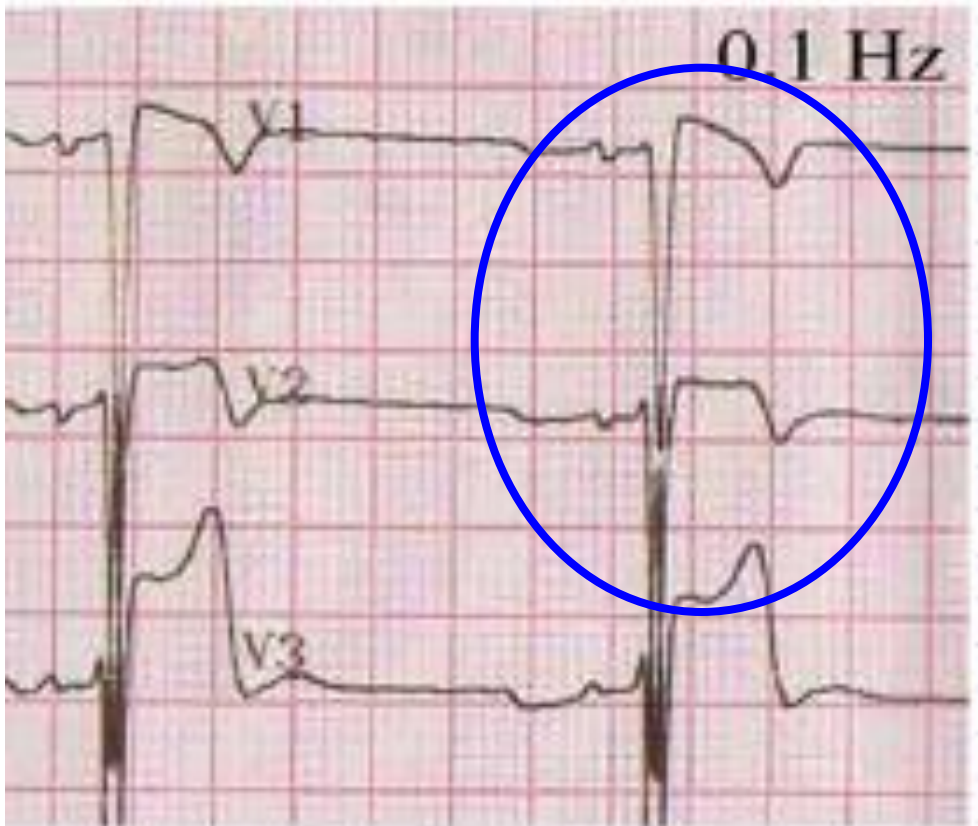


# Simulation of anteroseptal myocardial infarction by electrocardiographic filters



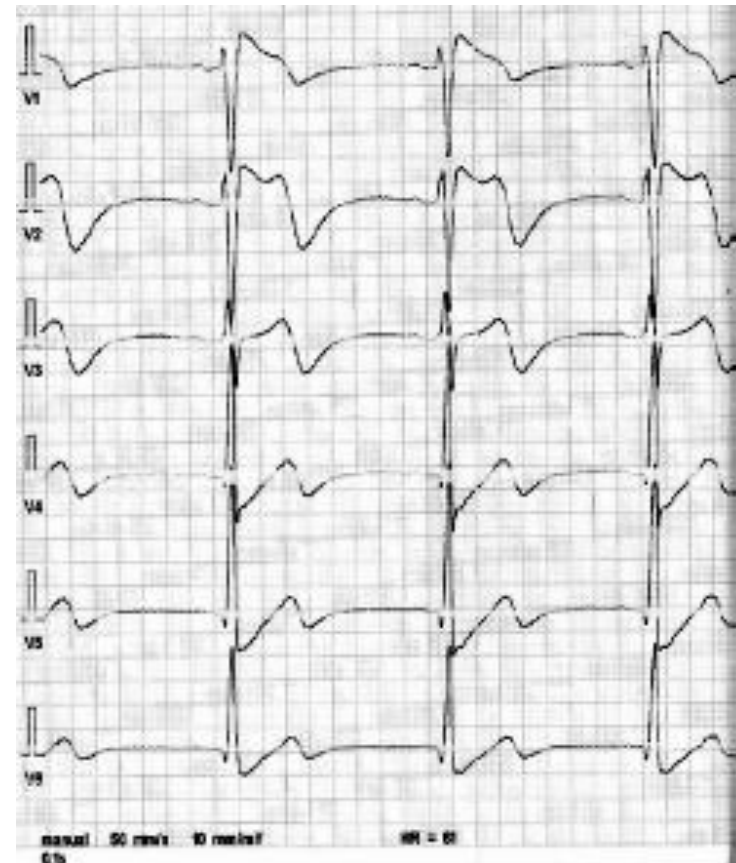
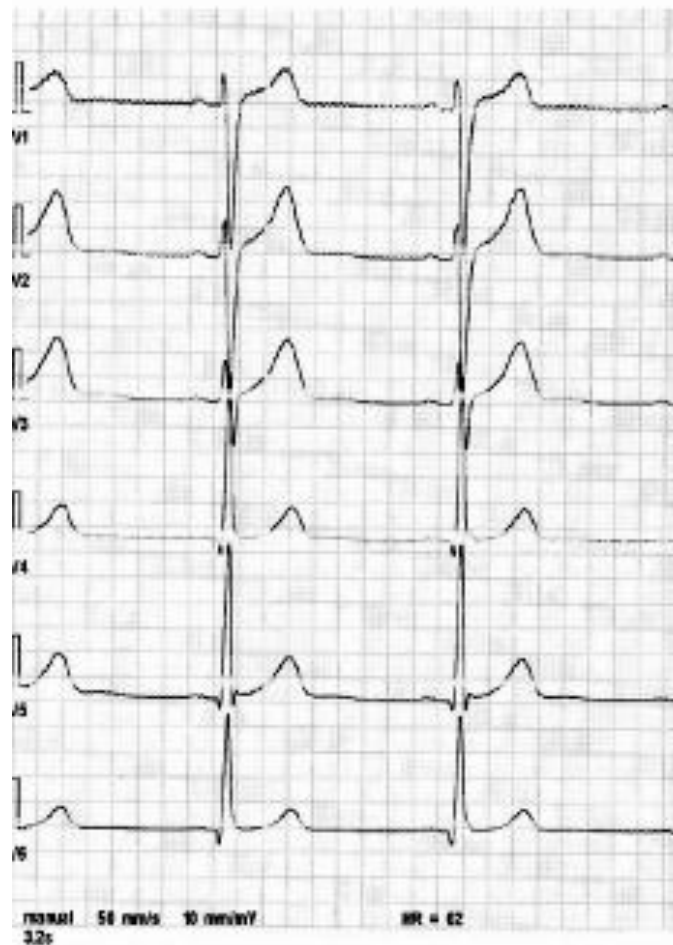
# Brugada electrocardiographic pattern: Reality or fiction?

Javier García-Niebla, RN,<sup>a,\*</sup> Guillem Serra-Autonell, MD,<sup>b</sup>  
Miquel Fiol, MD, PhD,<sup>c</sup> Antonio Bayés de Luna, MD, PhD<sup>d</sup>



# Nieprawidłowe ustawienie filtrów czy zespół Brugadów?

Abnormal filter setting or Brugada syndrome?



# I filtri: problemi tecnici

- **This distortion results from phase nonlinearities that occur in areas of the ECG signal where frequency content and wave amplitude change abruptly, as occurs where the end of the QRS complex meets the ST segment. Digital filtering provides methods for increasing the low-frequency cutoff without the introduction of phase distortion.**

# I filtri: problemi tecnici

- This can be accomplished with a bidirectional filter by a second filtering pass that is applied in reverse time, that is, from the end of the T wave to the onset of the P wave.
- This approach can be applied to ECG signals that are stored in computer memory, but it is not possible to achieve continuous real-time monitoring without a time lag.

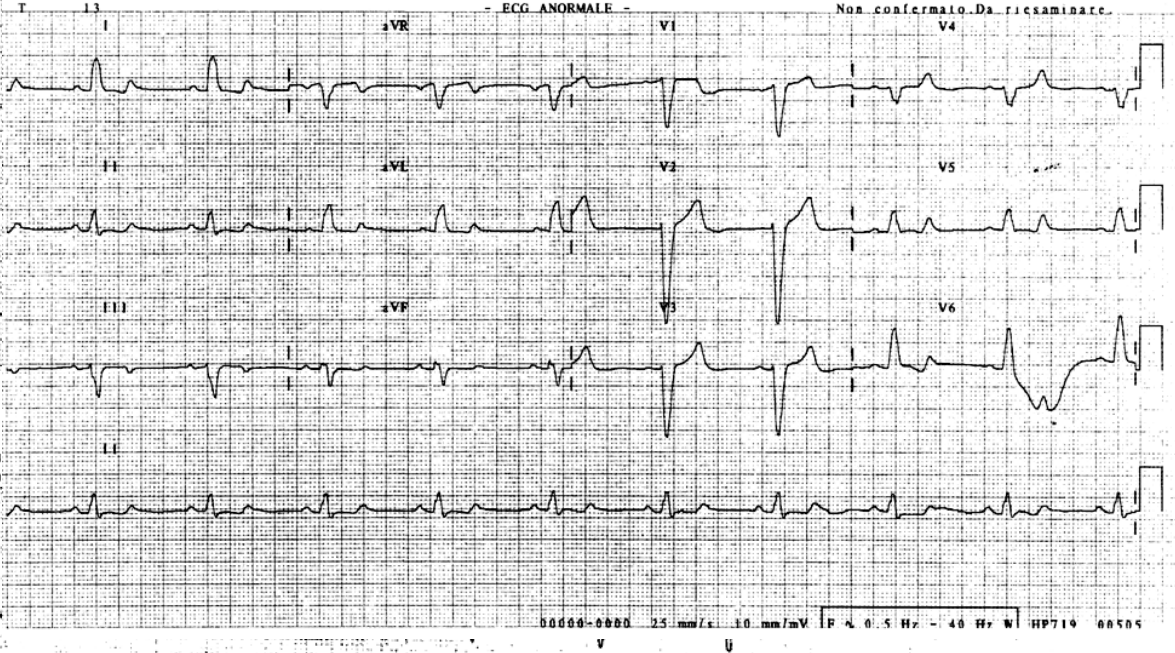
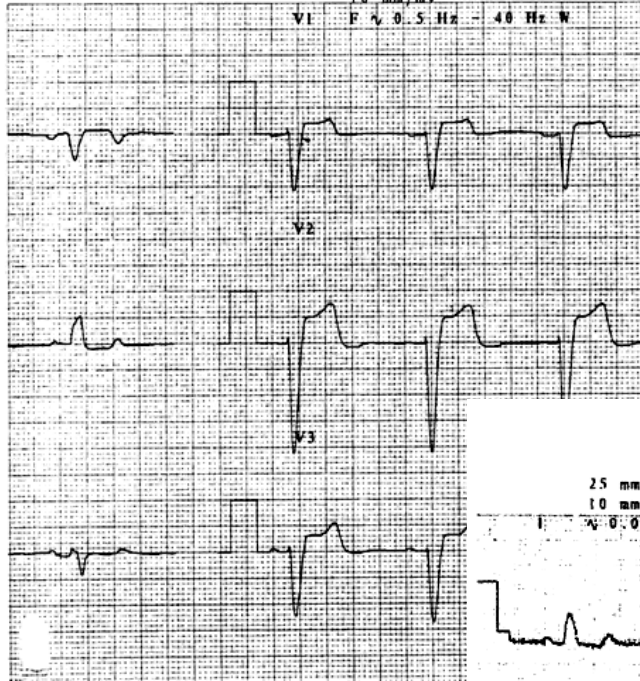
MAN Tolleranza

Freq. 58 . ETA' NON INSER., PRESUM. 50 ANNI PER INTERPR. ECG  
 PR 168 . RITMO SINUSALE NORMALE, FREQUENZA 58.....ASSE P. PR. FREQ. E RITMO NORMALI  
 ORSD 137 . BLOCCO DI BRANCA SINISTRA (BBS).....ORS>120. R AMPIA/CON INCIS.. I-V6  
 QT 434  
 QTc 426

--Asse--  
 P 38  
 ORS -11  
 T 13

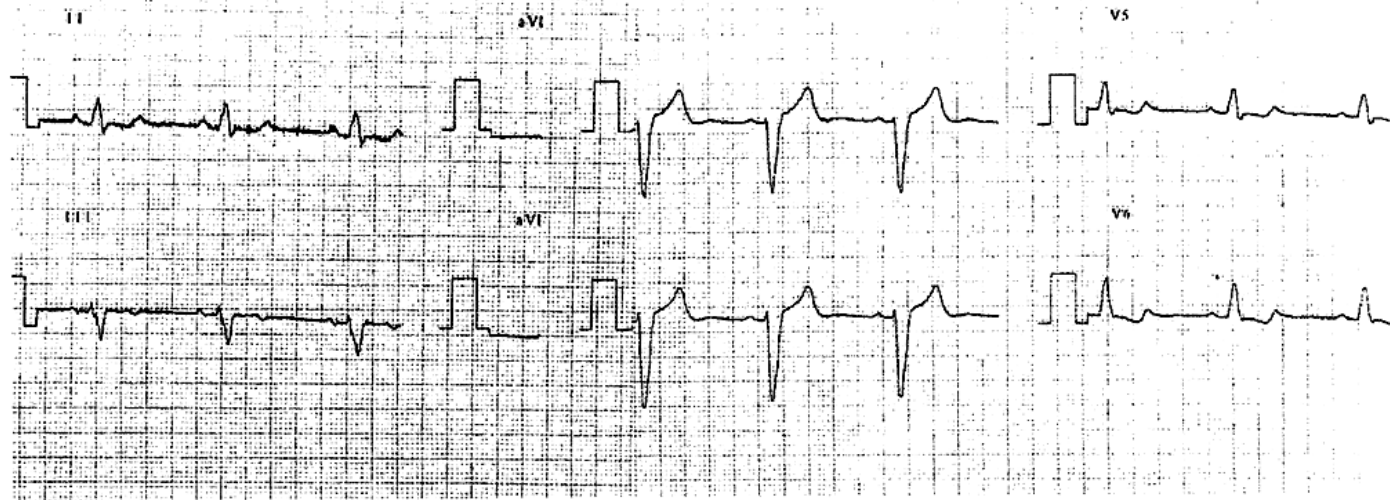
25 mm/s  
 10 mm/mV

VI F v 0.5 Hz - 40 Hz W



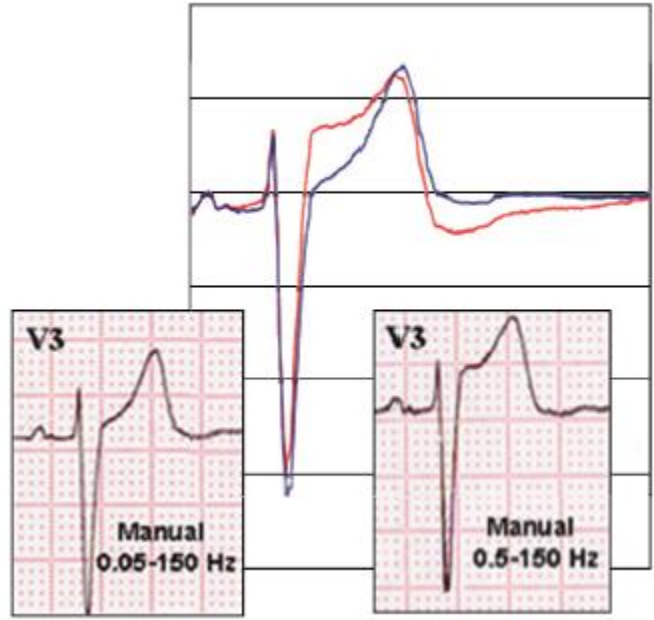
25 mm  
 10 mm  
 W 0.0

0000-0000 25 mm/s 10 mm/mV P v 0.5 Hz - 40 Hz W HP719 00505

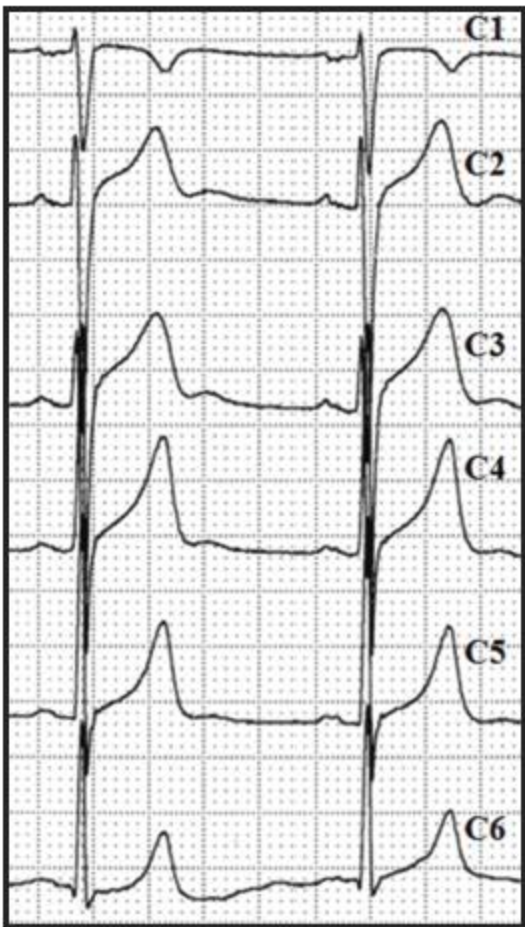




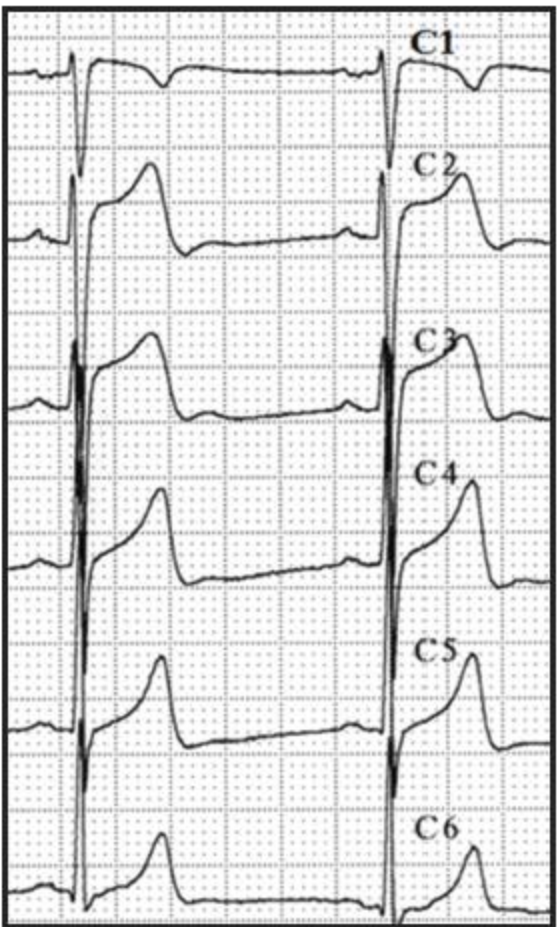
# High-Bandpass Filters in Electrocardiography: Source of Error in the Interpretation of the ST Segment



# High-Bandpass Filters in Electrocardiography: Source of Error in the Interpretation of the ST Segment

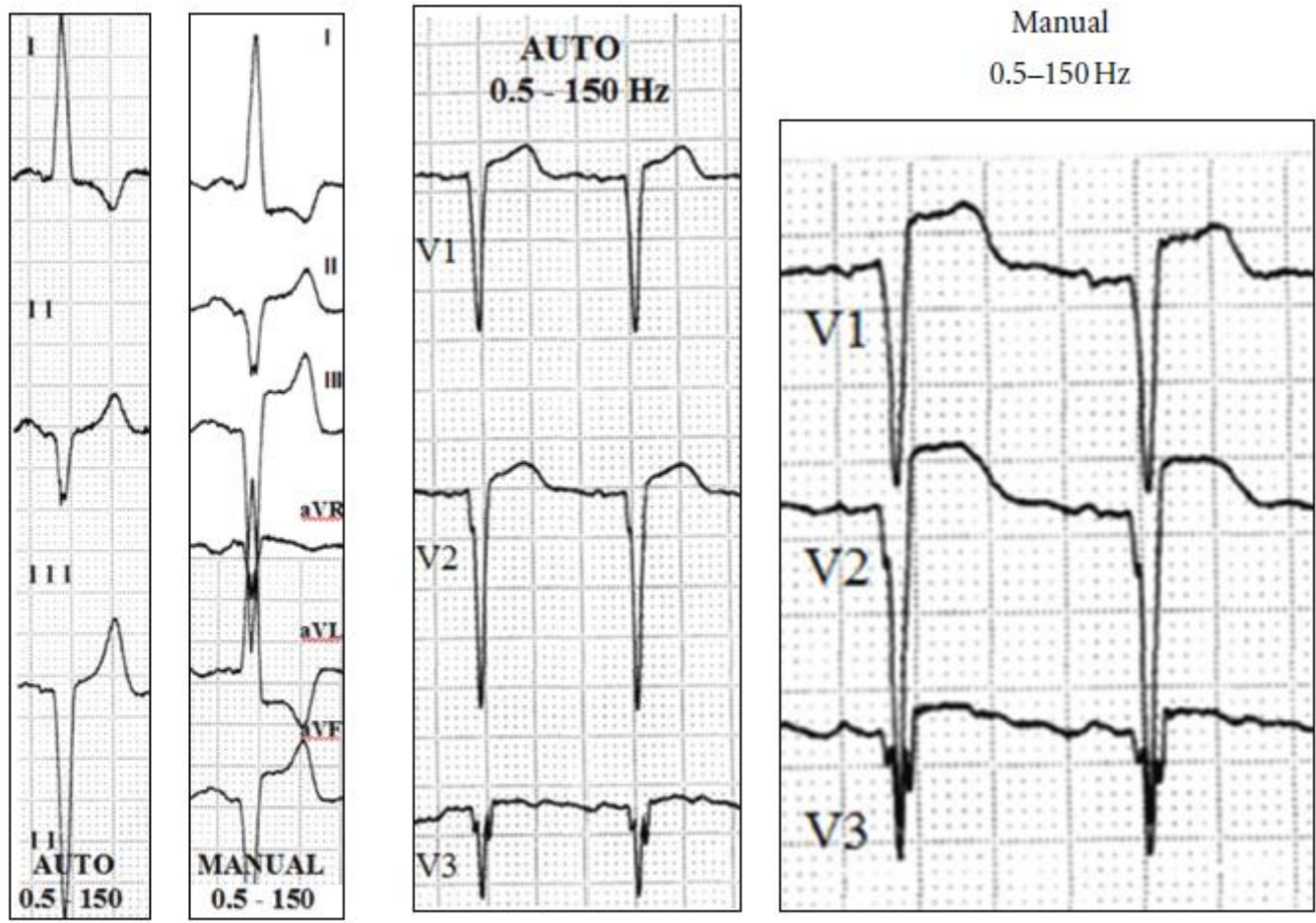


Auto (0.5-150 Hz)



Manual (0.5-150 Hz)

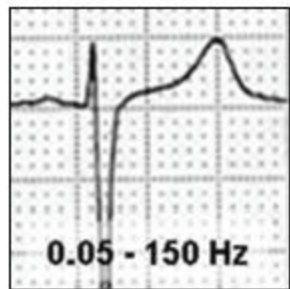
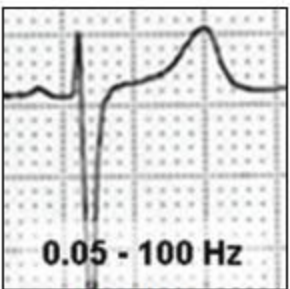
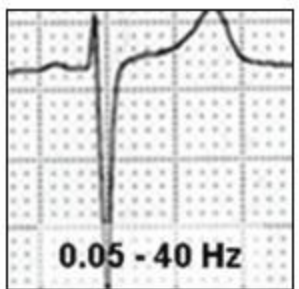
# High-Bandpass Filters in Electrocardiography: Source of Error in the Interpretation of the ST Segment



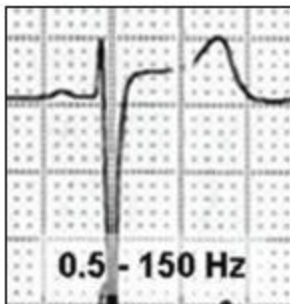
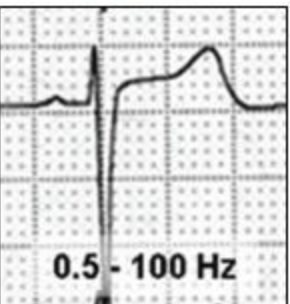
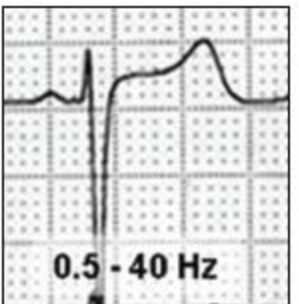
(a)

# High-Bandpass Filters in Electrocardiography: Source of Error in the Interpretation of the ST Segment

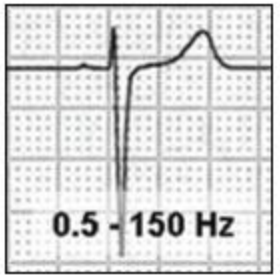
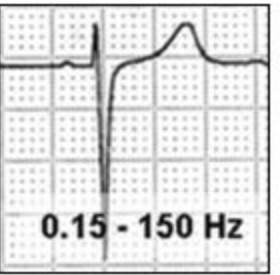
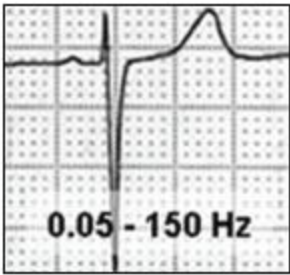
Manual



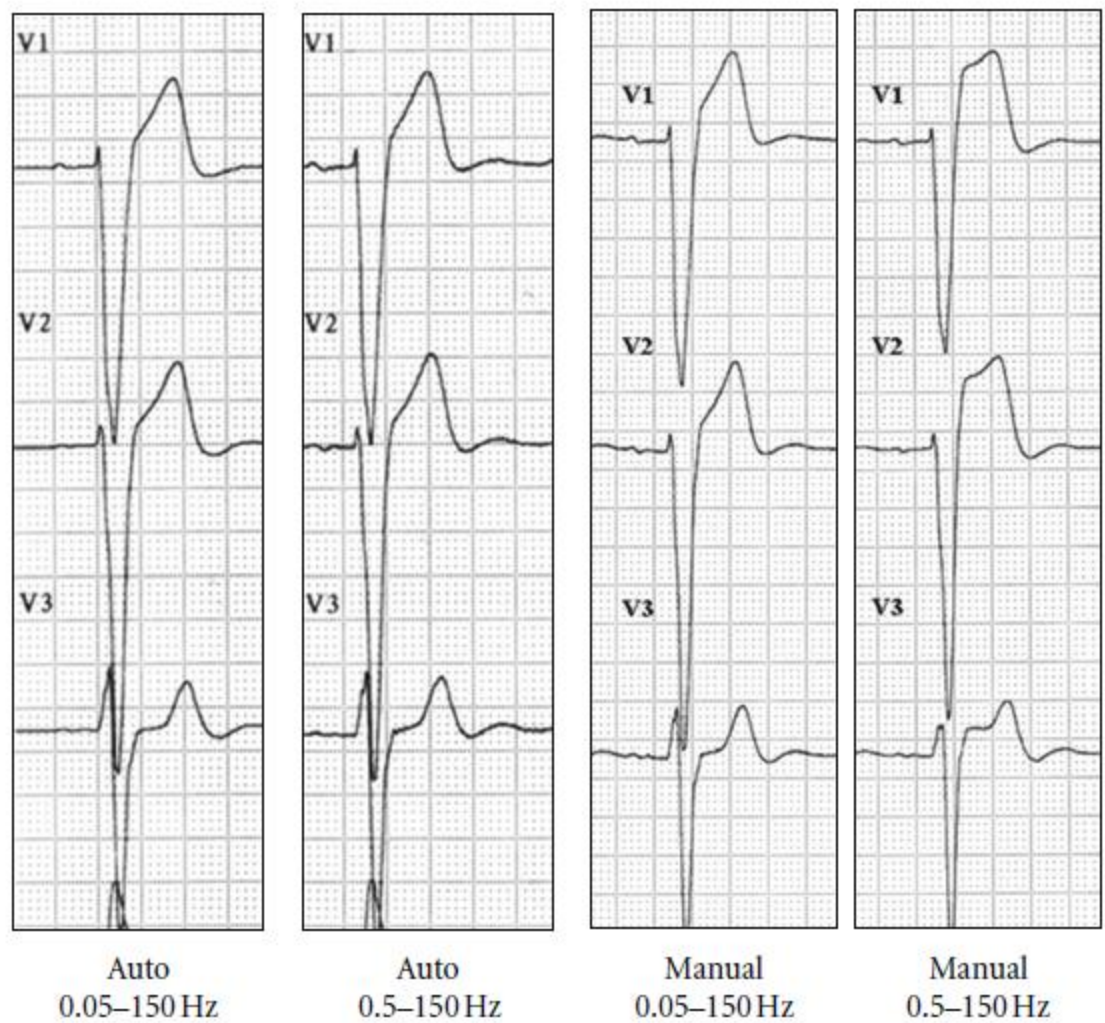
Manual



Auto



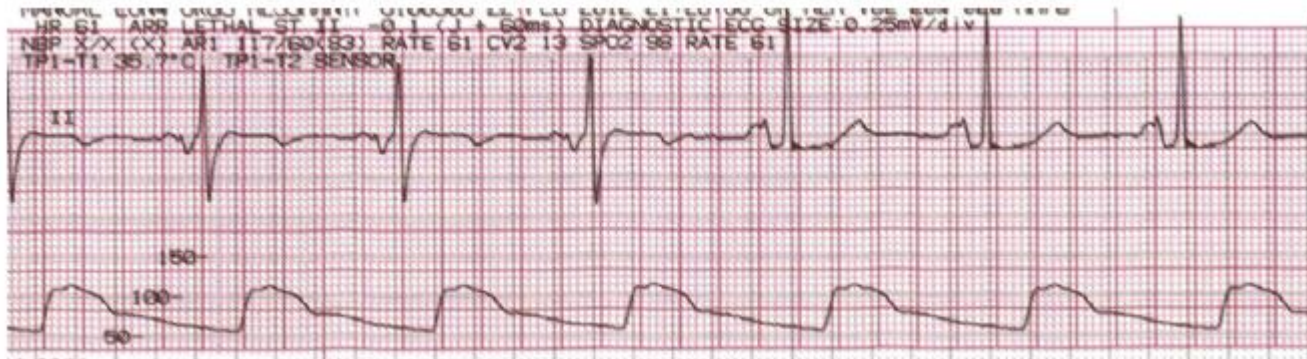
# High-Bandpass Filters in Electrocardiography: Source of Error in the Interpretation of the ST Segment



# I Filtri

- **Low-frequency noise, such as that produced by respiration, causes the tracing to wander above and below the baseline. A low-frequency cutoff at 0.5 Hz, which was once widely used in ECG rhythm monitors, reduces baseline drift due to the generally lower frequency of respiratory motion but can result in marked distortion of repolarization that may produce artifactual ST-segment deviation.**

# Reflections on an Electrocardiogram: Inverted T Waves



# Recommendations for the Standardization and Interpretation.....

## High-Frequency Filtering

digital sampling must be performed at twice the rate of the desired high-frequency cutoff.

Because this theorem is valid only for an infinite sampling interval, the 1990 AHA report recommended sampling rates at 2 or 3 times the theoretical minimum.

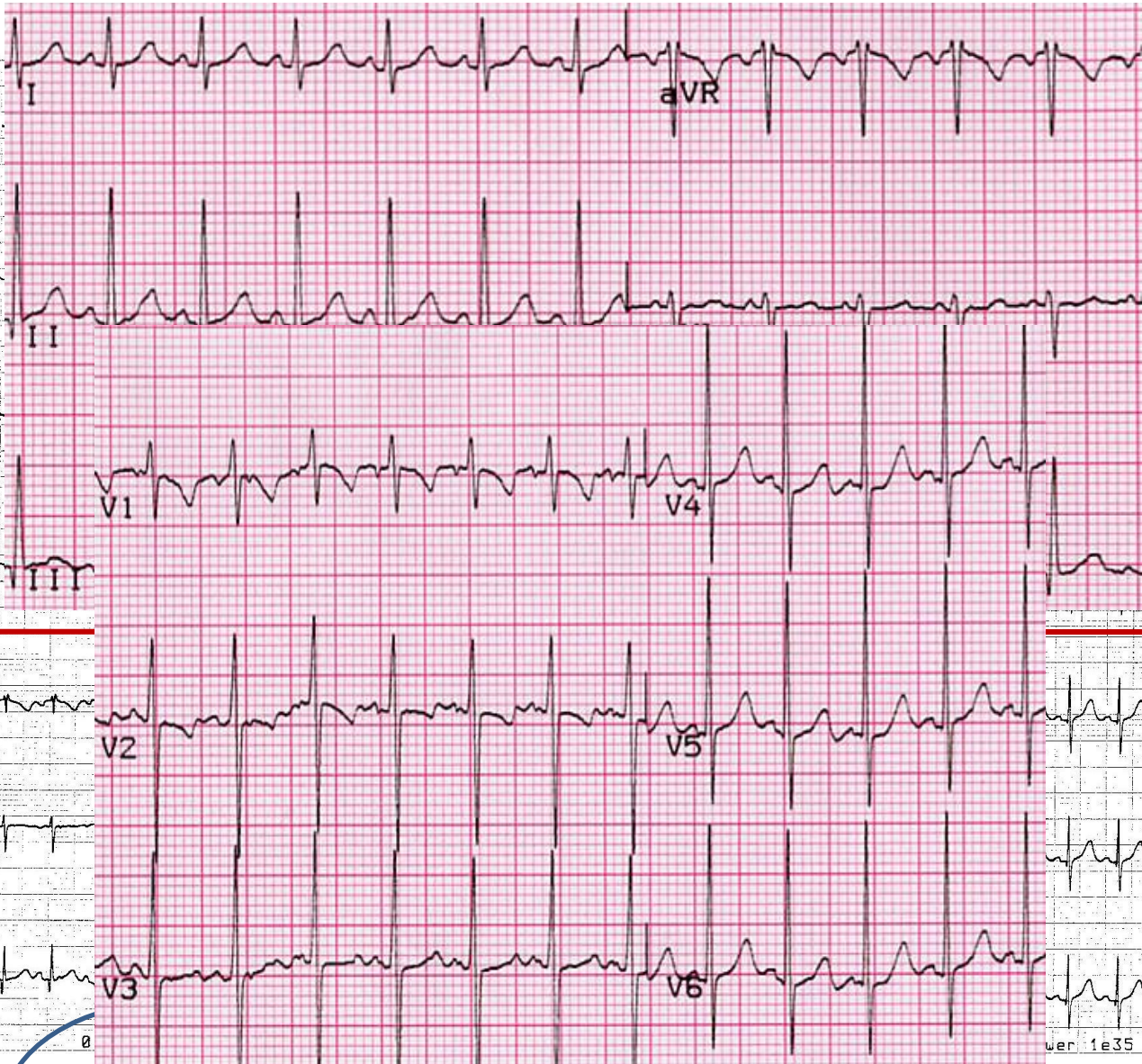
Data at 500 samples per second are needed to allow the 150 Hz high-frequency digital filter cutoff that is required to reduce amplitude error measurements to circa 1% in adults



# **Recommendations for the Standardization and Interpretation.....**

- The higher the frequencies contained in the filtered signal, the more accurate will be the measurement of rapid upstroke velocity, peak amplitude, and waves of small duration.**
- Inadequate high-frequency response reduces the amplitude of QRS measurements and the ability to detect small deflections.**
- A high-frequency cutoff of 100 Hz was considered adequate by the AHA in 1975 to maintain diagnostic accuracy during visual inspection of direct-writing tracings by electrocardiographers.**

ESTERNO  
13.02.2014  
1 mesi



25 mm/s

0.05 -35 Hz

wer 1e35 Mm

## Recommendations for the Standardization and Interpretation.....

- An obvious consequence of these high-frequency recommendations is that reduction of noise by setting the high-frequency cutoff of a standard or monitoring ECG to 40 Hz will **invalidate any amplitude measurements used for diagnostic classification.**
- The standard of 1991, reaffirmed in 2001, recommended a high-frequency cutoff of at least 150 Hz for all standard 12-lead ECGs

**Table 1 ECG Criteria**

Model (Ref. #)	Criteria	
Sokolow-Lyon voltage (17)	$SV_1 + RV_5/V_6 \geq 3.5$ mV and/or $RaVL \geq 1.1$ mV	
Sex-specific Cornell voltage (18)	$SV_3 + RaVL > 2.8$ mV (for men) and $> 2.0$ mV (for women)	
Romhilt-Estes point score (19)	Diagnostic $\geq 5$ points and probable $\geq 4$ points	
	<b>Criteria</b>	<b>Points</b>
	Voltage criteria	
	R or S wave in limb leads $\geq 20$ mm	3
	S wave in $V_1$ or $V_2 \geq 30$ mm	3
	R wave in $V_5$ or $V_6 \geq 30$ mm	3
	ST-T wave abnormality	
	ST-T vector opposite to QRS complex without digitalis	3
	ST-T vector opposite to QRS complex with digitalis	1
	Negative terminal P wave in $V_1$ 1 mm in depth and 0.04 s in duration	3
	Left axis deviation	2
	QRS duration $\geq 0.09$ s	1
	Delayed intrinsicoid deflection in $V_5$ or $V_6$ ( $> 0.05$ s)	1
Perugia score (20)	Positivity of $\geq 1$ of the following 3 criteria: $SV_3 + RaVL > 2.4$ mV (men) or $> 2.0$ mV (women), left ventricular strain, or Romhilt-Estes score $\geq 5$	
Perugia 2 score (21)	Positivity of $\geq 1$ of the following 2 criteria: $SV_3 + RaVL > 2.4$ mV (men) or $> 2.0$ mV (women), or left ventricular strain	
Minnesota code 3.1 (22)	$RV_5/V_6 > 2.6$ mV or $RI/II/III/aVF > 2$ mV or $RaVL > 1.2$ mV	
Lewis index (23)	$[(RI + SIII) - (RIII + SI)] > 1.7$ mV	
Framingham-adjusted Cornell voltage (24)	men: $[RaVL + SV_3 + 0.0174 \times (\text{age} - 49) + 0.191 \times (\text{BMI} - 26.5)] \geq 2.8$ mV; women: $[RaVL + SV_3 + 0.0387 \times (\text{age} - 50) + 0.212 \times (\text{BMI} - 24.9)] \geq 2.0$ mV	
Cornell voltage product (25)	$([RaVL + SV_3] \times \text{QRS duration}) \geq 243,600$ $\mu\text{Vms}$	
Sokolow-Lyon voltage product (25)	$(SV_1 + RV_5/RV_6) \times \text{QRS duration} \geq 371,000$ $\mu\text{Vms}$	
Gubner and Ungerleider voltage (26)	$RI + SIII \geq 2.2$ mV	

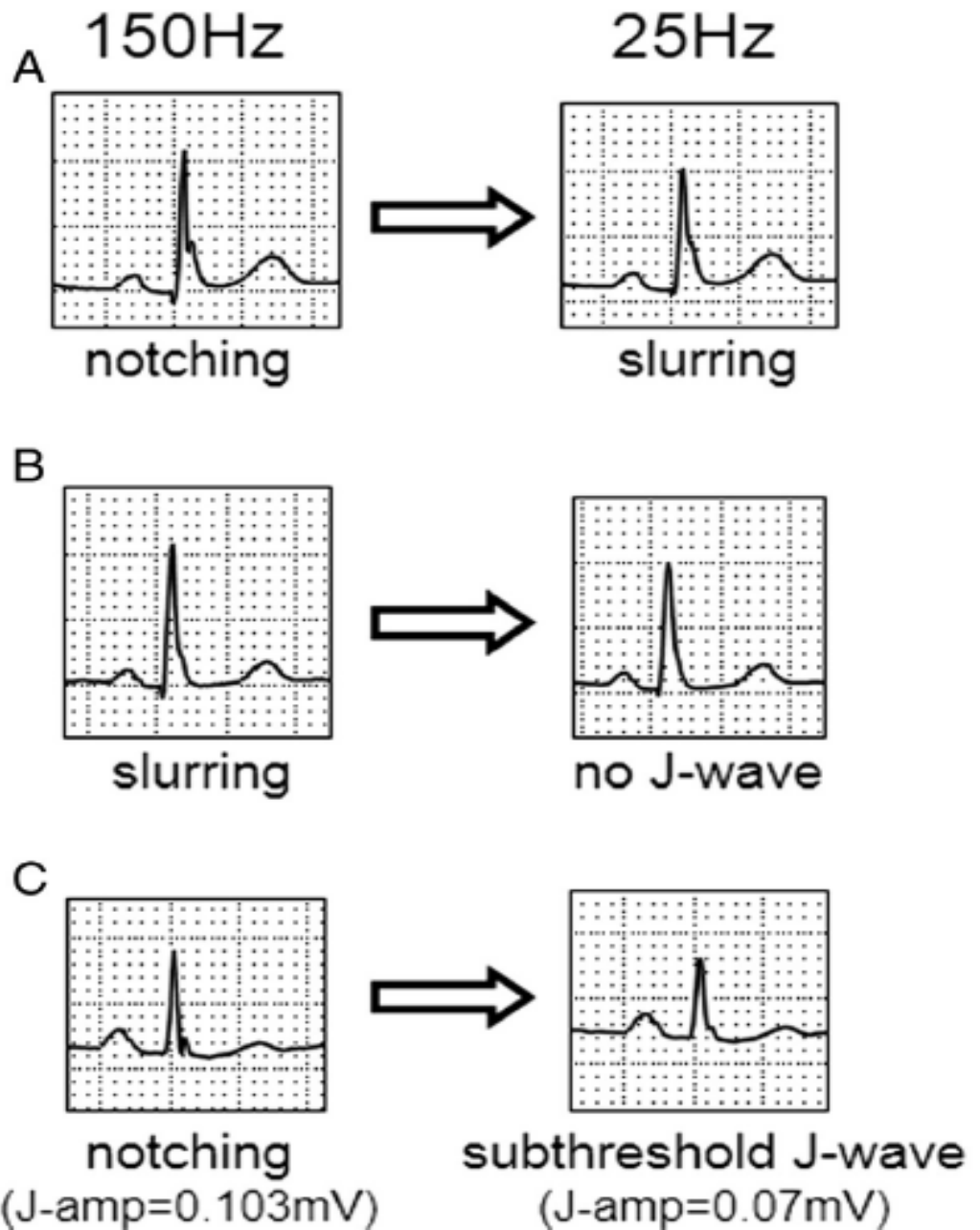
## **Recommendations for the Standardization and Interpretation.....**

- **Greater bandwidth may be required for accurate determination of amplitudes in infants.**
- **The European CSE group recommended that waveforms should be recognized if they have amplitudes of at least 20 $\mu$ V and durations of at least 6 ms.**
- **This implies a high-frequency response in the range of 150 Hz. A 2001 Dutch report showed that in order to keep amplitude errors  $\approx$ 25  $\mu$ V in >95% of the cases, a bandwidth up to 250 Hz is needed for pediatric cases and up to 150 Hz for adolescents**

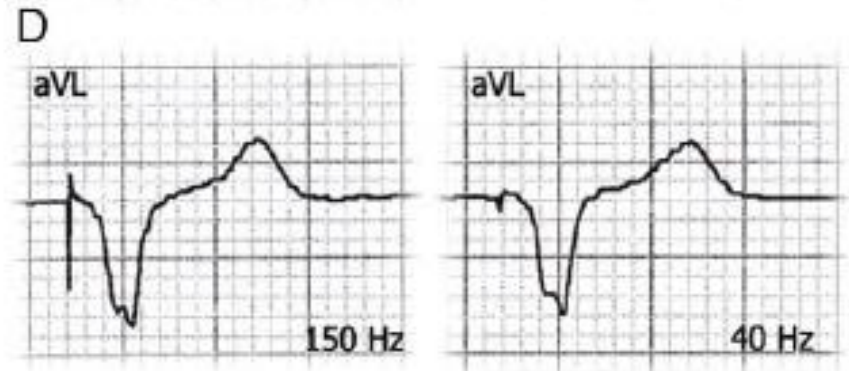
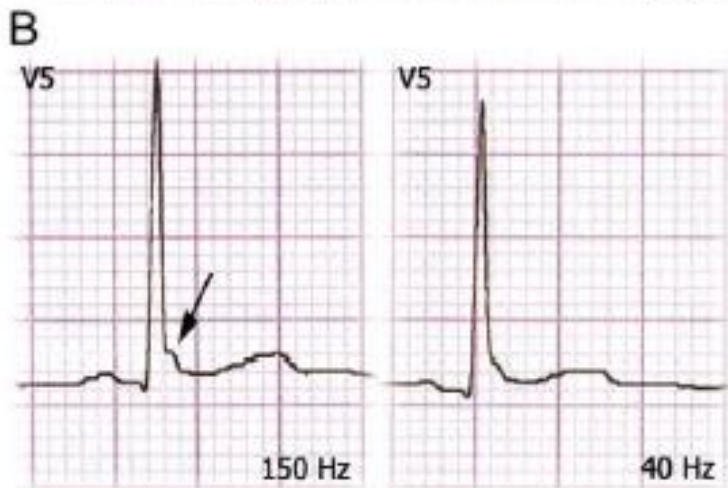
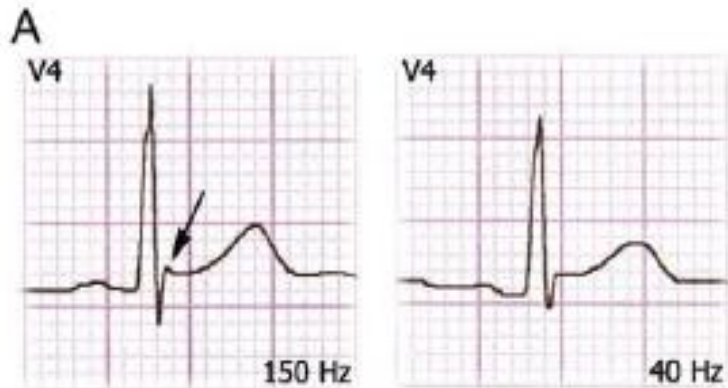
## **Recommendations for the Standardization and Interpretation.....**

- Even so, it has long been recognized that higher-frequency components of the QRS complex are present and that these components may have clinical significance in patients with various forms of heart disease.**
- To measure routine durations and amplitudes accurately in adults, adolescents, and children, an upper frequency cutoff of at least 150 Hz is required; an upper frequency cutoff of 250 Hz is more appropriate for infants**

# Effect of ECG filter settings on J-waves



## Effects of inadequate low-pass filter application





- Oversampling was originally introduced to detect and represent pacemaker stimulus outputs, which are generally circa 0.5 ms in duration. Front-end sampling has been performed at rates from 1000 to 2000 per second, but newer converters can routinely sample at 10 000 to 15 000 per second or even higher;

20.08.1943

Maschio

70 anni

..... cm / .....

..... kg

FC 127/min

Asse e...

Intervalli:

P 0°

RR 474 ms

QRS 76°

P 70 ms

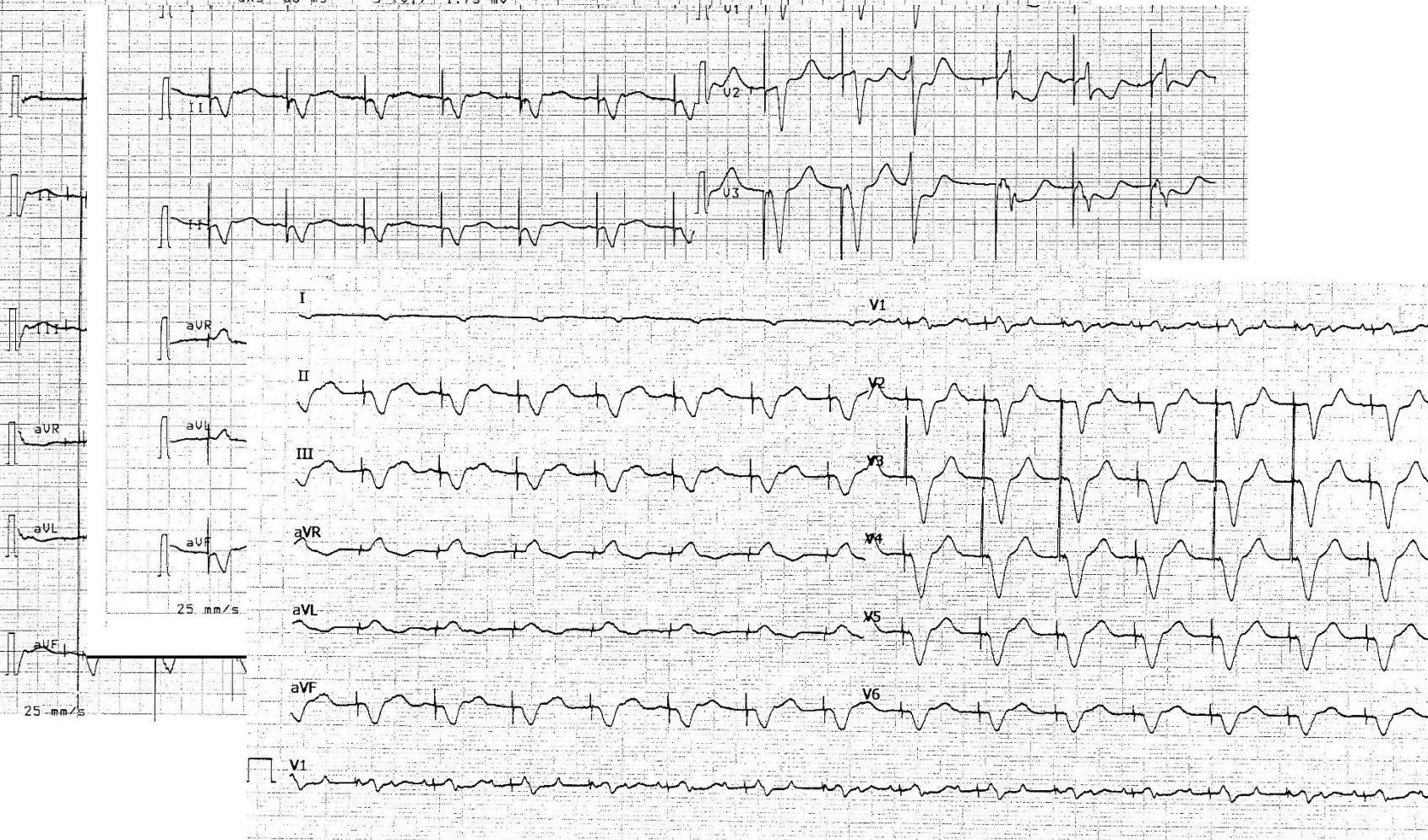
T -97°

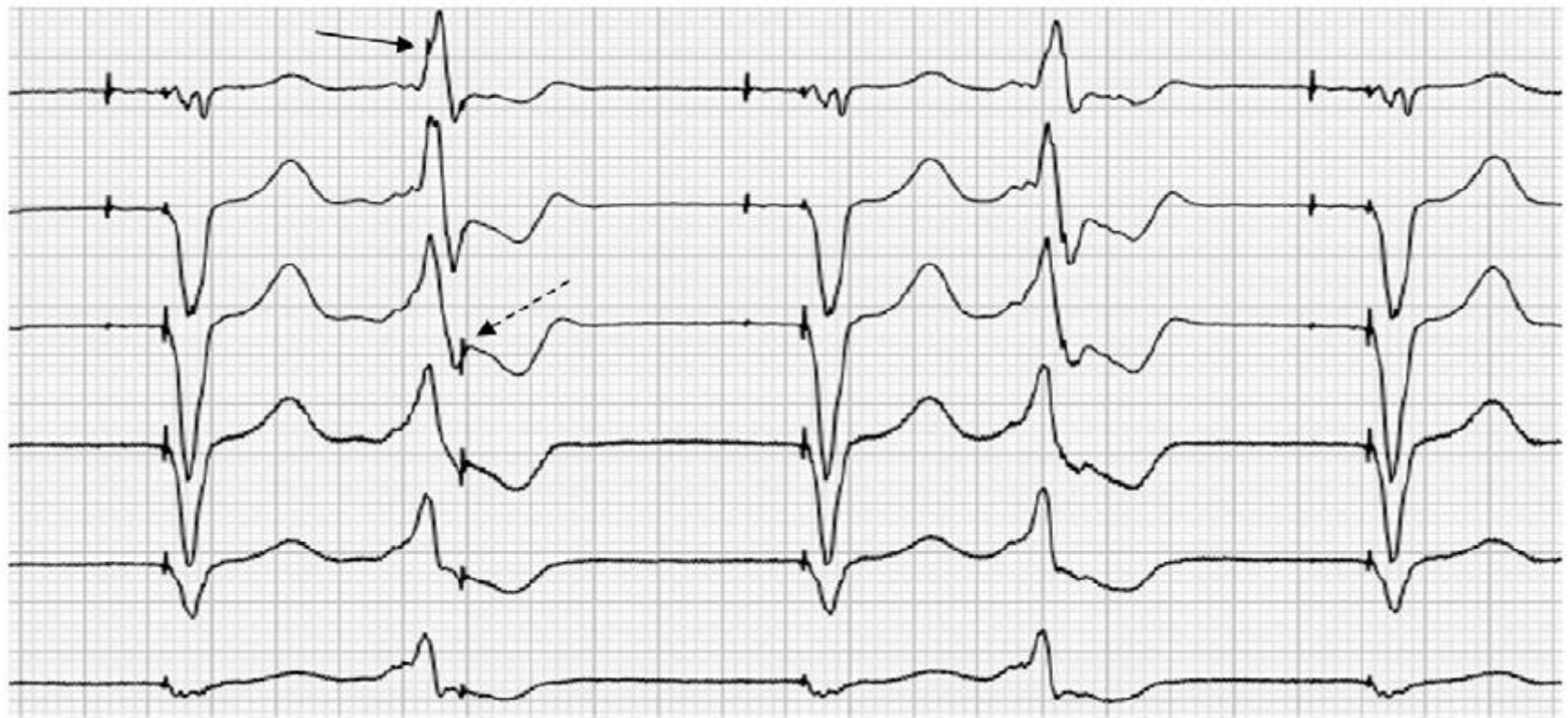
PD 92 ms

P (II) mV

QRS 68 ms

S (V1) -1.73 mV





## **Impact of Pacing and High-Pass Filter Settings on Ventricular Bipolar Electrograms in Implantable Cardioverter Defibrillator Systems**

**– Implication of Predictors for Inappropriate Therapy Caused by Oversensing of Repolarization Electrograms –**

**The R wave amplitude during DDD was significantly lower as compared to that during the other conditions in all high-pass filter settings.**

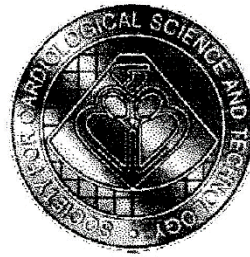
**The existence of Brugada syndrome and T/R ratio during the AAI with a high-pass filter setting of 10/20 Hz was an excellent predictor of T wave oversensing in the follow-up period.**

**DDD had a significant impact on the R wave amplitude reduction and the T/R ratio during AAI can be predictors of T wave oversensing. These findings have important implications for inappropriate shocks due to T wave oversensing.**

# **Recommendations for the Standardization and Interpretation.....**

- **The 1975 AHA recommendations included a 0.05-Hz low-frequency cutoff for diagnostic electrocardiography. This recommendation preserves the fidelity of repolarization, but it does not eliminate the problem of baseline drift.**
- **To reduce artifactual distortion of the ST segment, the 1990 AHA document recommended that the low-frequency cutoff be 0.05 Hz for routine filters but that this requirement could be relaxed to 0.67 Hz or below for linear digital filters with zero phase distortion.**
- **These standards continue to be recommended.**

- **These most recent limits continue to be recommended for adolescents and for adults, with extension of the high-frequency cutoff to 250 Hz in children.**
- **Electrocardiographs should automatically alert the user when a suboptimal high-frequency cutoff, such as 40 Hz, is used, and a proper high-frequency cutoff should automatically be restored between routine standard ECG recordings.**



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## **Clinical Guidelines by Consensus**

**Recording a standard 12-lead electrocardiogram**

**An Approved Methodology**



February 2010  
Review Date: February 2013

## Appendix C: AUDIT CHECKLIST

### Filter Settings

1. In 'Auto' mode is the machine preset to a recording bandwidth of either: 0.05Hz – 100Hz or 0.5Hz – 100Hz?  
 Yes       No
2. In 'Manual' or 'real time mode' is the machine preset to a recording bandwidth of 0.05Hz – 100Hz?  
 Yes       No
3. Is the mains filter (50Hz) set to 'off'?  
 Yes       No

### Training

1. Has the person performing the ECG recording been appropriately assessed in this technique?  
 Yes       No



## Recording

1. Are the patient details present and correct?  
 Yes       No
2. Is the ECG free of artefact?  
 Yes       No
3. If artefact is present has an explanation been written on the ECG?  
 Yes       No       N/A
4. Has the mains filter been used?  
 Yes       No
5. If the front panel 'filter' has been selected has an explanation been written on the ECG?  
 Yes       No       N/A
6. Have the appropriate gain settings been used?  
 Yes       No
7. If the rhythm is irregular has an additional rhythm strip been recorded?  
 Yes       No       N/A

## Guidelines for recording a standard 12-lead electrocardiogram

### Equipment

- Electrocardiograph that meets or exceeds the requirements of IEC 60601-2-51 (2003)\*.

The device should be pre-programmed in accordance with American

\* IEC 60601-2-51 (2003) - *Particular requirements for safety, including essential performance, of recording and analysing single channel and multichannel electrocardiographs*. This document establishes minimum safety and performance requirements for electrocardiographic (ECG) systems that are intended for use in the analysis of rhythm and of detailed morphology of complex cardiac complexes.

\*\* Digital filter design allows for the low-frequency filter to be raised to **0.5Hz** when recording in 'auto' mode. However, ST-segment distortion may occur when this setting is used in 'manual' mode. Fixing the low-frequency setting at **0.05Hz** in the pre-set should prevent this error occurring<sup>3</sup>.

\*\*\* AAMI EC12-00 (2000) - This standard establishes minimum labeling, safety, and performance requirements for disposable electrodes used for diagnostic electrocardiography.

'Manual' or 'real time' mode      0.05 Hz – 40 Hz

- Disposable tab electrodes that meet or exceed the requirements of AAMI EC12-00 (2000)\*\*\*\*
- Skin preparation equipment (for example, razor, abrasive tape)